Pulsatile Load-Dependent Strain Rate Modulates Aortic Tissue Viscoelasticity exvivo

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INTRODUCTION	RESULTS	CONCLUSION
Central aortic tissue is continuously exposed to cyclic pulsatile stretching. Previous data indicated that increased	** A [] B [] C **** *** ***	There are significant differences in viscoelastic properties between segments from distinct anatomical

pulsatile load reduced both rigidity and arterial vascular (VSMC) cell smooth muscle contractility, suggesting a potential causal relationship VSMC function between and pulsatile load-controlled tissue stiffness. In the present study, the effect of pulsatile load on arterial physiology was further investigated.



regions along the aortic tree, especially when comparing thoracic and abdominal aortic tissue. Pulsatile load (either via pulse frequency or via pulse modulates the pressure) viscoelastic properties of the arterial wall due to, in part, strain rate-dependent effects.

NEXT STEPS

Whereas increased strain rate softening strain causes in aortic tissue *vivo*, its ex mechanism is not yet fully known. Studying which viscous and/or elastic component(s) are affected by strain rate could physiological reveal new mechanisms. Additionally, the cellular responses to these mechanical stimuli could be to identify the investigated involved vascular mechanotransduction pathways.



Figure 1. Pulse pressure modulates the pressure-stiffness relationship. (Neutel et al., 2021)

Figure 3. Viscoelastic properties along the aortic tree. (A) The IA has a significantly higher E_p than both the AA (p<.01) and DA (p<.01). (B, C) Additionally, the IA has both a significantly higher E_{η} and E_{E} than the AA (p<.001; p<.0001) and the DA (p<.001; p<.001). There was no difference in viscoelastic parameters between the AA and the DA. Data is expressed as mean ± SEM, n=4, One-way ANOVA with Holm-Sidak post hoc test for multiple comparisons. *p<.01, **p<.001, ***p<.0001. $E_p =$ Peterson's Elastic Modulus, E_n = Viscous Modulus, \dot{E}_E = Elastic Modulus, $A\dot{A}$ = Ascending Aorta, $D\dot{A}$ = Thoracic Descending Aorta, **IA** = Abdominal Infrarenal Aorta



METHODS

Aortic segments from C57BL/6J (n=4) mice were mounted in the ROTSAC, and subjected to high frequency cyclic stretch. Diastolic and systolic diameter as well as the Peterson modulus $(\mathsf{E}_p),$ as a measure of aortic stiffness, were determined. The viscous (E_n) and elastic modulus (E_E) extracted from were pressure- diameter tracings by eliminating loop hysteresis.



Figure 4. Pulse pressure and pulse frequency modulate blood vessel viscoelasticity. (C) Increasing pulse frequency (from 10 Hz to 25 Hz) decreased Ep in all vascular tissues. (A, B) Increasing pulse frequency (from 1 Hz to 25 Hz) decreased E_n , but increased E_E . (C) Increasing pulse frequency (from 10 Hz to 25 Hz) decreased Ep in all vascular tissues. Increasing pulse pressure (10 mmHg to 100 mmHg) decreased (D) E_n and (F) Ep. (E) A biphasic response of the E_E was observed when increasing pulse pressure. Datà is expresséd as mean \pm SEM, n=4. E_p = Peterson's Elastic Modulus, E_n = Viscous Modulus, E_E = Elastic Modulus, AA = Ascending Aorta, DA = Thoracic Descending Aorta, IA = Abdominal Infrarenal Aorta.



Figure 6. Increased strain rate induces (strain) softening of vasular tissue. How strain rate affects the viscoelastic of the arterial wall, components responsible for this effect, is not fully known. Identifying which viscoelastic components are affected, could reveal dependent strain-rate vascular mechanotransductive pathways.



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Figure 2. Rodent Oscillatory Tension Set-up for measuring Arterial Compliance (ROTSAC). (Leloup et al, 2016)

Figure 5. Strain rate is inversly correlated with the stiffness and the viscous properties of the **ascending aorta**. (A) An increase in strain rate is significantly (p<.0001) inversly correlated with the E_p . (B) Increased strain rate is significantly (p<.0001) inversly correlated with E_n . (C) There was no correlation between strain rate and E_E in this dataset. E_p = Peterson's Elastic Modulus, E_n = Viscous Modulus, E_E = Elastic Modulus

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